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Invincible, but Not Invisible: Imaging Approaches Toward In Vivo Detection of Cancer Stem Cells

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A B S T R A C T

With evidence emerging in support of a cancer stem-cell model of carcinogenesis, it is of paramount importance to identify and image these elusive cells in their natural environment. The cancer stem-cell hypothesis has the potential to explain unresolved questions of tumorigenesis, tumor heterogeneity, chemotherapeutic and radiation resistance, and even the metastatic phenotype. Intravital imaging of cancer stem cells could be of great value for determining prognosis, as well as monitoring therapeutic efficacy and influencing therapeutic protocols. Cancer stem cells represent a rare population of cells, as low as 0.1% of cells within a human tumor, and the phenotype of isolated cancer stem cells is easily altered when placed under in vitro conditions. This represents a challenge in studying cancer stem cells without manipulation or extraction from their natural environment. Advanced imaging techniques allow for the in vivo observation of physiological events at cellular resolution. Cancer stem-cell studies must take advantage of such technology to promote a better understanding of the cancer stem-cell model in relation to tumor growth and metastasis, as well as to potentially improve on the principles by which cancers are treated. This review examines the opportunities for in vivo imaging of putative cancer stem cells with regard to currently accepted cancer stem-cell characteristics and advanced imaging technologies.

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INTRODUCTION

Clonal evolution, the classic and widely accepted model of carcinogenesis, attributes tumor growth to a single cell's acquiring a combination of genetic mutations resulting in unlimited proliferation.1-3 This model suggests that maintenance and progression of tumors occurs by continual selection of the strongest and most resistant cells within the tumor. Therefore, every cell within a tumor has the potential to acquire the proper mutations to become invasive and/or metastatic. The cancer stem-cell (CSC) model of carcinogenesis was initially described in the context of liquid malignancies in the 1930s and has recently garnered attention with regard to solid tumors.^{1,4} In contrast to that of clonal evolution, the CSC theory maintains that cancers develop from, and are maintained by a CSC arising from a resident normal stem/progenitor cell within the tissue bearing the malignancy. The theory holds that the CSC arises from either a stem cell with genetic or epigenetic mutations resulting in the cancer phenotype or from a transformed progenitor cell that also acquires the stem-cell ability of selfrenewal. CSCs possess the ability to produce progeny of both stem-cell and differentiating fates, resulting in tumors of a heterogeneous phenotype.^{4,5} In addition, recent evidence suggests that stem cells are the culprits of metastasis,⁶ supported by the observation that metastatic tumors tend to reproduce a similar heterogeneity as the primary tumor.⁷ Furthermore, CSCs from solid tumors have been identified as chemo- and radioresistant, pointing to their potential role in recurrence.⁸⁻¹² Therefore, the CSC model suggests that the true culprit for tumor maintenance and metastasis could possibly lie in the ability of CSCs to survive microenvironmental challenges, resist genotoxic chemotherapy and radiation therapy, repopulate the tumor through unlimited rounds of proliferation, and maintain CSC numbers through asymmetric division.

CSCs are a rare population of cells, making up as little as 0.1% of cells in primary specimens and cell lines tested.⁹ A low target number is of therapeutic advantage as long as chemotherapy and radiation are effective in killing CSCs. Unfortunately, an ever-growing body of publications suggests that the opposite is true. CSCs are resistant to genotoxic chemotherapeutics (via increased drug pump activity and/or their slow doubling time) and radiation therapy (possibly by increased DNA repair activity).^{8,10-14} The CSC model raises the concern that treatments targeting rapidly proliferating and/or non–stem-like cells are

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destined to fail.¹⁵ Therefore, the ability to identify and quantify CSCs has therapeutic and possibly even prognostic value. Currently, the gold standard in confirming the identification of a CSC population requires serial passage of the cells in vivo. These assays are difficult to perform, but have led to the identification of a CSC population in brain, breast, skin, prostate, lung, and colon cancers (Table 1). The ability to use identified markers of CSCs for in vivo imaging is of utmost value for expanding our knowledge of CSC function and translating such knowledge to clinical use.

Identification and purification of the CSC population from clinical samples and cell lines has proven successful when based on the expression of a particular combination of cell-surface markers,¹⁶⁻²² as well as by functional assays including the exclusion of the Hoechst-33342 DNA-binding dye (the "side population"),²³⁻²⁶ or the presence of increased aldehyde dehydrogenase activity.²⁷ There exists a small body of knowledge regarding the differential gene expression patterns of CSCs; however, the identification of CSCs on the basis of the expression pattern of particular genes has yet to be described, with the exception of a recent publication by Liu et al²⁸ describing a relationship between the loss of BRCA1 expression and an increased stem/ progenitor phenotype in human breast cancer patients. Nevertheless, such an identification method is certainly capable of being exploited for the in vivo imaging of CSCs. In addition, information regarding CSC biology can be obtained by imaging CSCs in conjunction with microenvironmental probes, such as markers of angiogenesis or protease activity.

With regard to the choice of imaging equipment, cellular resolution is a primary concern. Optical fluorescence imaging provides the highest resolution to date; however, magnetic resonance imaging (MRI) and positron emission tomography (PET) are making advancements in spatial resolution that warrant their inclusion in this review.²⁹⁻³¹ Considering that the CSC population will be as low as one cell among 1,000, the imaging device must be sensitive to the contrast agent at a resolution on the order of 100 nm. This necessity all but excludes use of the VisEn FMT (VisEn Medical, Woburn, MA), the Explore Optix (GE/ART, Montreal, Quebec, Canada), the Odyssey (LI-COR Biosciences, Lincoln, NE), the Maestro (CRi, Woburn, MA), and the popular IVIS (Xenogen/Caliper, Hopkinton, MA), while still

Type of Cancer	Stem-Cell Marker	Expression Level	References
Breast	CD44	Positive	16
	CD24	Negative/low	16
	lin	Negative	16
	ALDH	High activity	27, 28
Brain	CD133	Positive	94, 95
Colon	CD133	Positive	20, 21
Prostate	CD44	Positive	6, 17
	α2β1	High	17
	CD133	Positive	17, 22
Acute myelogenous leukemia	CD34	Positive	93
	CD38	Negative	93
	CD96	Positive	18
Pancreas	CD44	Positive	19
	CD24	Positive	19
	ESA	Positive	19

including basic imaging devices, such as a dissecting microscope outfitted with a Nuance imaging module or other high-resolution imagers (CRi, Woburn, MA; Table 2, Fig 1A). The ability to image CSCs in vivo will provide novel information regarding the biology of these cells in the presence of a stromal compartment, microenvironmental cues, and most importantly, in three dimensions. As clinical trials are altered to include measurements of stem-like cells, the imaging of CSCs in vivo will provide a powerful tool to translate CSC biology into clinical application by driving the development and testing of CSC-specific therapies, prognostic indices, and measures of therapeutic efficacy.

IMAGING CSCs IN HUMAN TISSUES

To best appreciate the approaches for imaging CSC populations in vivo, we will first highlight data using ex vivo human specimens from which such approaches are extrapolated. As already mentioned, the ability to simultaneously image cellular antigens and functional markers of CSCs is of great value. This has been explored in vitro within a range of cell lines and tissues by a number of laboratories,^{28,32,33} as well as with animal and human specimens ex vivo.^{28,34-36} In addition, similar studies have also gathered information with regard to tissue organization and the distinct localization of subpopulations of cells, such as stem cells.³⁷⁻⁴⁰ Two-photon fluorescence has contributed useful information as to cellular organization in both two-dimensional cultures⁴¹ and three-dimensional reconstruction of xenografted tumors.⁴² The use of multiple contrast agents necessitates the ability to differentiate spectral profiles and remove background signal. Therefore, the spectral unmixing of multispectral images has proven powerful in the detection of rare subsets of cells within cell lines, spheroid cultures, and tumor sections. Perhaps the most elegant example of this is the discrimination of human mesenchymal stem cells from osteoblasts by seven-color fluorescence and spectral unmixing performed by Schieker et al.⁴³ Because CSCs are identified by increasing numbers of markers, the need for imaging seven markers at once is not difficult to foresee. In addition, Byers et al⁴⁴ have demonstrated elegant multispectral imaging by performing gene expression profiling with oligonucleotide probes (labeled with quantum dots) in conjunction with immunohistochemistry, as a means of semiquantitative, highthroughput analysis of cellular lineage and gene expression patterns in human tissues. Interestingly, Chung et al⁴⁵ have employed optical imaging to demonstrate unique cancer profiles in terms of spectral reflectance and autofluorescence measurements without the use of exogenous contrast agents. These types of in vitro analysis provide important information regarding the discrimination of CSCs from neighboring cancer cells within a cell line or tumor. In addition, it is easy to envision the use of such analyses as a means of determining the prognosis of cancer patients via CSC numbers in bone marrow, blood, CSF, or tumor biopsies, a strategy already being explored.^{35,46,47}

IN VIVO IMAGING OF CSCs

Established Imaging Models

The imaging of cancer cells at single-cell resolution is not a novel undertaking. Rather, it is the in vivo imaging of CSCs specifically that remains to be accomplished. On the basis of convincing reports thus

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Table 2. Comparison of the Specifications of High-Resolution Optical Imaging Devices					
Criterion	OV100*	IV100*	Nuance/Nikon AZ100†	Multiphoton Laser Scanning Microscopy	
Hardware					
Numerical aperture Camera pixels Magnification	0.03-0.43 4080×3072 (DP70 CCD*) 0.14×-16×	0.14-0.7 64×64-4096×4096 6×-27×	0.05-0.5 1434×1050 (Sony ICX285)‡§ 5×-400×	Approximately 1.2 512×480§ 60×	
Surgical manipulation					
Subcutaneous	Skin flap	Very small incision	Skin flap or excised	Excised	
Internal organ	Skin flap	Small skin flap/incision	Skin flap or excised	Excised	
Advantages	4 individual parcentered and parfocal lenses; spectral unmixing; NIR	3 simultaneous detection channels for fluorescence; 4 lasers; NIR	Spectral unmixing; NIR	Lack of out-of-focus absorption; low excitation light scatter; NIR	
Abbreviation: NIR, near *Olympus, Center Valle †Nikon, Tokyo, Japan. ‡Sony, Tokyo, Japan. §Varies according to c	r-infrared. ey, PA. amera chosen.				

far, CSCs should be a high priority of oncologic imaging studies. Multiple publications in the last decade have successfully imaged cancer cells at single-cell resolution under ex vivo conditions, as well as longitudinally for studies of tumor growth and response to therapy.⁴⁸⁻⁵² In 1997, Chishima et al⁵³ imaged micrometastases ex vivo with an MRC-600 confocal imaging device mounted on a Nikon microscope. They orthotopically implanted GFP-expressing CHO-K1 ovarian cells and identified GFP-positive micrometastases in the excised lungs and liver of the mice. Nonproliferative lung micrometastases of GFP-expressing breast tumor cells have also been imaged ex vivo following mammary fat pad injection.⁵⁴ In 2000, Chen et al⁵⁰ published a longitudinal study detecting fluorescent neurons at singlecell resolution with two-photon laser scanning microscopy. Initial cellular tracking studies evolved into fluorescence reporter assays by establishing cell lines with specific promoter-driven fluorescent proteins, such as that of Fukumura et al,55 whereby vascular endothelial growth factor transcriptional activity was measured in response to microenvironmental factors in orthotopic brain tumors in vivo. In addition to gene expression imaging profiles, MRI and PET imaging techniques provide a functional component that can be more readily applied in clinical translational studies. Both MRI and PET have recently advanced to become more accessible for high-resolution needs,⁵⁶ and therefore, are discussed further in this review.

In addition to specifically tracking cells of interest via fluorescence or other agents of contrast, a number of physiological probes have been developed to image tumor microenvironmental events, such as angiogenesis, protease activity, and apoptosis. Injection of the blood pooling agent Angiosense (VisEn Medical) results in tumorspecific accumulation over time, likely a result of the leaky nature of tumor vasculature. VisEn also provides tumor-associated protease probes, MMPSense reporting matrix metalloproteinase activity (MMPs 2, 3, 9, and 13), ProSense, which is activated by Cathepsins B, L, and S, and plasmin within the extracellular milieu of solid tumors, and the osteogenic probe OsteoSense. Many studies have taken advantage of these physiological indicators.⁵⁷⁻⁵⁹ The tracking of apoptosis has also been successful with Annexin V probes that bind cells with extracellular phosphatidylserine exposure, and are therefore valuable in monitoring therapeutic response, albeit with limitations.^{60,61} Tracking rare cells, such as CSCs, in conjunction with microenvironmentspecific probes will be useful in providing additional information as to the behavior of the cells of interest under specific environmental conditions. Imaging a rare population of cells on the basis of gene expression, biochemical activity, or cell surface protein levels is possible with current knowledge of CSC characteristics. Additional microenvironment-specific CSC survival and growth patterns will be revealed when imaged in vivo, and the influence of other components of the tumor microenvironment such as hypoxia or pH changes can be determined.

High-Resolution Optical Imaging

For the purpose of imaging at the resolution of a single cell, optical imaging techniques are most readily applicable to the CSC model. When optically imaging a rare population of cells, the choice of both reporter signal and imaging device are equally important. With regard to the choice of optical signal, a fluorescent signal provides the greatest advantage at visualizing small numbers of cells. Despite the success with which bioluminescent signals define tumor growth, regression, and metastasis, the spatial resolution and sensitivity limitations of bioluminescence render it incapable of identifying and localizing rare cells at high resolution or with tomographic capability. Luciferase reporter plasmids have been extremely valuable at providing measurements of biologic activity in growing tumors with high sensitivity; however, luciferase models require animals to be injected with, and every cell in question be exposed to, the luciferin substrate. Furthermore, the limitation of the signal in vivo requires expression of luciferase in at least 2,500 cells for proper detection.⁶² Therefore, for the purposes of imaging a very rare population of cells, such as CSCs, readout of fluorescence is the ideal choice. The detection of fluorescence is made practical by the high intensity and stability of signal, the highly sensitive detectors available, and the option to concurrently employ more than one fluorophore. There is a large variety of potential fluorophores from which to choose, including fluorescent proteins such as GFP, RFP, YFP, and DsRed, the DsRed variant fruit fluorescent proteins such as mCherry,⁶³ cyanine fluorochrome conjugates, quantum dots and probes,44 and chimeric transmembrane fluorescent proteins,⁶⁴ and others. As already described, the ability to



Fig 1. High-resolution fluorescence imaging of CD133⁺ putative cancer stem cells in a live population of SW620 human colorectal carcinoma cells. (A) Photograph of the Nuance module (CRi, Woburn, MA) mounted on a Nikon AZ100 dissecting microscope (Nikon, Tokyo, Japan). (B) Phase contrast image of SW620 cells, and (C) spectrally unmixed image of CD133⁺ cells (green) and live cells counterstained with MitoTracker Red (Molecular Probes, Eugene, OR).

image fluorescent cells in vivo at high resolution has been demonstrated by many labs with models requiring relatively minor adaptations for the specific visualization of CSCs.

In terms of imaging technology, there are a number of optical imaging devices capable of high-resolution optical imaging, including the OV100 and IV100 imagers (Olympus, Tokyo, Japan), multiphoton laser scanning microscopes, Cellvizio (Mauna Kea Technologies/ Leica, Paris, France), and the relatively simple yet effective set-up of a dissecting microscope (such as a Nikon AZ100; Nikon, Tokyo, Japan) equipped with the Nuance multispectral imaging module (CRi). Each of these devices provides high-resolution imaging; the advantages of one over another merely stem from the particular objectives of the experiment at hand and cost of the equipment. Factors concerning the choice of imaging device include, but are not limited to, depth of tissue penetration, imaging time points, and option for multispectral unmixing. Depth of penetration is a significant factor in subcutaneous xenograft models and when imaging internal organs, whereby creation of a skin flap is necessary to avoid skin-associated light scatter. The IV100 is most advanced in this regard as the largest of the objectives is 3.5 mm in diameter allowing it to be easily inserted into small incisions (Table 2). The number of imaging time points desired is a significant factor because longitudinal studies with the OV100 and IV100 require incisions or transparent window models, but these are relatively easy to perform and have been demonstrated in many mouse models.⁶⁵⁻⁶⁹ In the absence of surgical manipulation, the highest penetration (with the least tissue damage) is achieved with near-infrared (NIR) fluorescence probes. Each of the imaging devices discussed here is capable of detecting signal in the NIR range. Depth of penetration and surgical manipulation become especially significant when longitudinal studies are desired. Multiple time points are not

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possible with multiphoton laser scanning microscopes, which are mainly useful for high-resolution end point analysis of excised tumors, but nonetheless provide valuable information. Lastly, the advantages of spectral unmixing are insurmountable. The unmixing feature allows for the removal of autofluorescence, as well as distinguishing between emission peaks of nominal separation. Autofluorescence is less of a complication with the IV100 or OV110 (because of the lasers' being narrowly focused on the specimen), but unmixing capabilities are a necessity for devices like the Nuance, where light scatter is more of a problem. Of course, considerations such as these are dependent on the model and end points chosen.

We have compared some of the instruments discussed based on important features of the hardware and prospective experimental design considerations (Table 2). Resolution is primarily dependent on the numerical aperture (NA) of the objective. NA is a value attributed to the ability of the objective to collect light and resolve detail at a fixed distance, with a higher NA value associated with better resolution. However, the final level of resolution achieved is also dependent on the magnification, the pixels of the image sensor, and the wavelength of the light. Each of the imaging devices listed is capable of cellular resolution, for example, using the OV100 MicroZoom objective with an NA of 0.43 (and with their DP70 CCD camera) will result in resolution of approximately 0.7 μ m. Also noted in Table 2 are the experimental limitations of the devices with regard to the manipulation of the specimen. It is possible for NIR fluorophores to penetrate the skin for imaging subcutaneous tumors, but to achieve the best images possible and for the imaging of internal organs each of the devices requires exposure of the tumor or organ in question. Various advantages specific to the imaging devices have also been highlighted in Table 2.

The Cellvizio instrumentation has introduced the capability to perform in vivo confocal microscopy during clinical GI endoscopy for visualization of tubular adenomas or Barrett's esophagus. A similar capability has been developed for imaging lung alveoli. It is not too difficult to imagine use of such capabilities or others for endoscopic or laparoscopic applications to visualize human CSCs in vivo.

High-Resolution MRI

Surprisingly, MRI is not to be left out of this discussion. Historically, MRI has been employed as a means of gaining anatomic information; however, recent advances in the evolution of contrast agents have provided the opportunity to image cells and gene regulation at cellular resolution with MRI.70 MRI image resolution is excellent, on the order of 100 μ m, but only recently has MRI technology been manipulated with the intent of detecting subtle molecular changes. By overexpressing an altered form of the transferrin receptor, Moore et al⁷¹ have increased the iron load within a target population of cells, thereby increasing contrast and detection. Similarly, Louie et al⁷² have engineered a beta-galactosidase reporter system in which cells with increased contrast are representative of transgene expression. These studies have succeeded in fusing the excellent in vivo detection capability of MRI with the cellular resolution and functional advantages of reporter activity. More recently, single-cell resolution imaging via MRI has successfully been employed to detect invading glioma cells and metastasizing breast carcinoma cells labeled with micrometersized particles of iron-oxide (MPIOs).^{29,30} Heyn et al³⁰ demonstrated high-resolution MRI of MPIO-labeled MDA-MB231BR/EGFP cells in the brains of mice at just 5 hours after intracardiac injection (Fig 2). They confirmed that the MRI signal voids were indeed the cells of interest by titrating the cell number and correlating the voids with fluorescent signal detected by high-resolution confocal microscopy. The noninvasive nature of MRI makes it one of the most attractive imaging techniques for longitudinal imaging. The possibility of noninvasive longitudinal imaging combined with the single-cell resolution models discussed make MRI a primary modality in the in vivo imaging of CSCs.

PET

PET quantitatively detects high-energy γ -rays emitted from a subject injected with positron-emitting isotopes or isotope-labeled molecular probes.73,74 PET is a sensitive and noninvasive imaging technique because the detection of positron emission is independent of the depth from which the signal is emitted. However, only modified PET instruments, such as those with pinhole and micropinhole apertures or micro-PET small-animal scanners are able to achieve resolution approaching (200 µm and/or 1 mm³) what is necessary for CSC imaging.⁷⁵⁻⁷⁷ PET technology is not yet at the level of resolution necessary for detecting single CSCs within a tumor; however, the level of spatial resolution has improved significantly, progress is being made in the development of radiolabeled antibodies, substrates, and reporter probes,⁷⁸⁻⁸⁰ and PET advancements are readily translated to the clinic. A common isotope-associated gene reporter system used with PET imaging is the detection of herpes simplex virus type 1 thymidine kinase (HSV1-tk) gene expression with an ¹⁸F-fluoropenciclovir probe, which when phosphorylated by HSV1-TK is retained within cells.^{80,81} In addition, Doubrovin et al⁸² have examined the regulation of endogenous genes with dual reporters for p53 and p21, resulting in the ability to simultaneously analyze the transcriptional activity of p53 and correlate those changes to effects on p21. PET strategies (via mutant HSV1-tk) have been combined with bioluminescence (via firefly luciferase expression) in an effort to image infused human mesenchymal stem cells with dual imaging modalities during bone formation and adipogenesis (Fig 3).⁷⁹ This is a potentially useful technique with the potential for adaptation to a CSC model to monitor the engraftment, propagation, and subsequent differentiation of CSCs at a primary or metastatic site. These studies highlight powerful capabilities of PET imaging that, when combined with the advantage of noninvasive detection, makes PET an attractive technique for imaging CSCs, with the requirement of further improvements in sensitivity and resolution. It is important to note there are two important goals: (1) human CSC tracking in vivo, which may be achieved by injecting ex vivo imaging agent-labeled cells and monitoring their fate over time in vivo; and (2) high-resolution imaging of endogenous human CSCs using exogenously administered, highly specific and sensitive probes. The second goal is the one that is extremely relevant to diagnostic and prognostic applications as well as the monitoring of the effects of therapy in patients.

NOVEL OPPORTUNITIES FOR IMAGING CSCs IN VIVO

Models that have proven successful for single-cell imaging include xenograft models of cells stably transfected with reporter constructs, transgenic mice, in vivo immunodetection of cell-surface proteins, and the application of exogenous probes or contrast agents. In applying what is currently known about CSCs, each of these models could

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Fig 2. Magnetic resonance detection of a single MPIO-labeled MDA-MB-231BR/ EGFP cells at day 0, and the effect of cell dose on the number of detectable cells are shown. (A) In vivo (100 \times 100 \times 200 μm^3) and (B) high-resolution ex vivo (100 μ m³) magnetic resonance imaging (MRI) of mouse brain demonstrates the presence of discrete signal voids (black arrow) throughout the brain of a mouse injected with 30000 Dragon Green MPIO and Dillabeled GFP+ cells. (C) A discrete signal void detected on MRI [black arrow in (A) and (B)] was correlated optically to a Dilpositive region (white arrow). Highresolution confocal microscopy revealed this region to be a solitary Dil-labeled cell (red) with green fluorescence attributable to either GFP expression or MPIO-labeled beads (inset of C). (D-F) In vivo MRI of mouse brains demonstrates the presence of increasing numbers of signal voids with increasing cell dose. Scale bar: (C) 500 μ m (inset, 10 μ m). Figure and legend reprinted with permission John Wiley and Sons Inc.30

be adjusted to specifically image CSCs. The CSC model exposes an important opportunity for the use of such techniques in characterizing the in vivo biology of CSCs and validating in vitro results. In vivo imaging of CSCs has yet to be explored beyond the realm of developmental biology, as much of what is known about the molecular signa-

ture of CSCs has been extrapolated from studies of normal stemcell biology.

For example, the polycomb repressive complex 1 (PRC1) protein Bmi-1 is involved in gene repression and is required for the maintenance of self-renewal in stem cells.⁸³⁻⁸⁵ Hosen et al⁸⁶ have generated a



Fig 3. Bioluminescence (BLI) of cube implants. BLI overlaid on (A) photograph and (B) radiograph. Both mice had six cubes: top two loaded with reporter-transduced human mesenchymal stem cells (hMSCs), middle two loaded with wild-type hMSCs, and bottom two loaded with empty-vector-transduced hMSCs located at caudal midline, and empty ceramic cubes located caudally and laterally. (C) Scanning electron micrograph of representative ceramic cube for cell loading and implantation. (D) BLI overlaid on radiograph in animal implanted with reporter-transduced hMSCs (top row, yellow arrow), mixture of emptyvector-transduced and reporter-transduced hMSCs (second row, green arrow), emptyvector-transduced hMSCs located at midline, and empty ceramic cube located laterally. Figure and legend reprinted with permission the Society of Nuclear Medicine.75

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Information downloaded from jco.ascopubs.org and provided by UNIV PENNSYLVANIA on June 6, 2008 from 130.91.205.241. Copyright © 2008 by the American Society of Clinical Oncology. All rights reserved. knock-in mouse under which GFP expression is regulated by the Bmi-1 transcriptional promoter to better understand the role of Bmi-1 signaling in the self-renewal mechanism. They found that Bmi-1 expression was highest within the most stem-like hematopoietic cells and was decreased on differentiation. This is an excellent example of a model system for studying stem cell-associated genes and should be expanded on to include an analysis of Bmi-1 regulation during tumor growth. Normal stem-cell imaging studies have also been performed in the context of Nestin⁸⁷ and Sox1⁸⁸ transgenic mice. Similar experiments can also be performed in mice bearing reporters of the Oct 3/4, Notch, Klf4, Sox2, BRCA1, NF-KB, and c-Myc genes, members of a short, but growing list of stem-cell and differentiation genes with potential roles in CSC function.^{28,89-92} In addition, such gene reporters can be generated under tissue-specific promoters in models of spontaneous tumor formation for a more detailed analysis of carcinogenesis with regard to tissue-specific stem-cell gene activity. These studies may lend invaluable information as to the true nature and/or existence of CSCs in growing tumors.

In addition to stem-cell gene regulation, the identification of cancerspecific stem-cell markers is of great value for in vivo imaging purposes. Similar to studies with the Annexin V probes, immunodetection of cellsurface markers with fluorophore-conjugated (or other isotope- or magnetic contrast-conjugated) antibodies is a great strategy for visualizing CSCs in the context of a growing tumor. CSC-specific cellular antigens have been identified for a number of tumor types (Table 1), particularly AML (CD96⁺ and/or CD34⁺/CD38⁻),^{18,93} breast (CD44⁺/CD24^{low/-}/ lin-negative),¹⁶ brain (CD133⁺),^{94,95} colorectal (CD133⁺),^{20,21} prostate $(CD44^+/\alpha 2\beta 1-high/CD133^+)$,^{17,22} and pancreas $(CD44^+/CD24^+/$ ESA⁺).¹⁹ Difficulty would be encountered when imaging cells with low- or negative-expressing antigens, but a combination of high expression of antigens could easily be detected with a variety of fluorophores and spectral unmixing capabilities. It is therefore possible to image prostate cancer cells expressing CD44, $\alpha 2\beta 1$, or CD133, and by definition, prostate CSCs expressing all three. In fact, we have recently imaged putative human CSCs within living SW620 human colon cancer cells with the Nuance module via preincubation with fluorescent-conjugated anti-CD133 antibody (Figs 1B-1C). The spectral unmixing feature of the Nuance allows for imaging of more than one cell-surface molecule given that different fluorophores are employed. In the example shown, Mito Tracker Red was used to document cell viability and the presence of viable CD133⁺ as well as CD133⁻ cells in the tumor cell population. Expanding on the identification of cell-surface proteins, LI-COR Biosciences has developed a probe to identify cells with epidermal growth factor receptor activity by labeling epidermal growth factor ligand with an NIR fluorophore. This represents a model system toward which the CSC field should be moving. The ability to identify new CSC-specific extracellular proteins will lead to the development of novel probes providing the opportunity to visualize CSCs in vivo, and possibly even therapeutically target⁹⁶ functional proteins necessary for CSC survival and resistance.

With regard to CSC-specific gene expression, there exists the option of imaging the functional characteristics of aldehyde dehydrogenase (ALDH) activity and dye efflux or retention in vivo. Both increased ALDH activity, efflux of Hoechst 33342, and retention of labeling dyes such as CFSE are functions associated with CSC populations; sorting cells on the basis of these characteristics enriches for tumorigenic CSCs.^{25,27,97,98} Although ALDH activity has only been measured under in vitro conditions, it is reasonable to envision the in vivo detection of ALDH concurrent with the identification of cellular antigens or biologic events such as angiogenesis. It is less likely that imaging Hoechst 33342 efflux in vivo would be practical; however, dye-retaining cells could potentially be visualized during tumor growth in vivo as long as the loss of dye does not precede measurable tumor burden. This would provide the opportunity to image the in vivo activity of quiescent cells with regard to the microenvironment. The alteration of organelle structure as a cell moves throughout capillaries⁹⁹ and the progression of a cell through the cell cycle in real time¹⁰⁰ have also been achieved and can be applied to our further understanding of CSC biology. These experiments relied on the tracking of specific proteins via fluorescence, a strategy that could be readily adapted to visualize the interplay between cells at differing levels of differentiation, and therefore expressing different cellular antigens in a dynamic manner. These suggestions, along with those regarding CSC gene expression, bring to light the possibility of imaging events more functional than the expression of cell-surface markers. However, it is likely that a combination of the imaging tools discussed herein will prove most useful in garnering novel information of in vivo CSC biology.

CLINICAL IMPLICATIONS FOR CSC IMAGING

With the ability to perform high-resolution imaging of CSCs comes new knowledge of CSC behavior in a relatively undisturbed environment compared with current in vitro models. Whether CSCs exist is still the subject of intense debate, hence use of the term "putative CSC." In vivo imaging of cancer cells thought to be stem-like will put to rest some of the unanswered questions pertaining to the CSC model, and potentially validate already accepted theories. Are CSCs the culprit of the well established chemo- and radioresistance of tumors? Monitoring CSC levels within a tumor responding to treatment would help to answer such a question. Do CSCs possess the metastatic ability within a tumor? With fluorescent- or MPIO-labeled CSCs it becomes possible to track the invasion and metastasis of very small numbers of cells.^{30,53,54,72} Similar questions are on their way to being answered in the clinic; however, the heterogeneous nature of patient populations makes it less likely that a consensus will be met in the next few years, as is possible with in vivo preclinical modeling.

Progress is being made in the development of prognostic measures of CSCs. Putative CSCs have been identified in the bone marrow of early breast cancer patients on the basis of the CD44⁺/CD24^{-/low} phenotype.35 In terms of clinical imaging advancements, Wang et al101 have successfully performed confocal optical imaging on colonic mucosa in human patients undergoing screening colonoscopy. They found that the movement pattern of fluorescein (applied topically within the colon) varies between normal and hyperplastic crypts, providing valuable real-time histologic analysis of cancer in vivo. Such studies could be modified to analyze CSC markers via optical imaging of fluorescently labeled antibodies during colonoscopy, and perhaps advancements in resolution MRI and PET imaging could also be employed. Such imaging techniques would produce a measure of the CSC component within primary tumors, lymph nodes, and sites of metastasis, thereby providing prognostic information as is already being explored ex vivo,^{35,46,47} and could potentially influence the therapeutic protocols for individual patients, as well as monitor therapeutic response during treatment. The human studies discussed require further characterization for the purpose of thoroughly assessing

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the factors driving cancer progression, metastasis, and CSC existence and behavior. However, these are excellent early steps in the identification and analysis of tumor cells at the single-cell level in living patients, and have the potential to drive the way in which CSCs are identified and quantified, prognoses are defined, and therapeutic strategies are developed.

SUMMARY

The recent high-profile reports describing the generation of pluripotent stem cells from fibroblasts raise the possibility that as few as four genes are required in maintaining the stem-cell phenotype.^{91,92} This observation lends support to the possibility that cancer arises from just a few mutations in resident tissue stem, progenitor, or even differentiated cells. It remains to be undeniably verified that CSCs are the sole culprit of carcinogenesis; however, in the study of CSC biology, highresolution imaging must be readily accessible because CSC biology requires analysis within the least manipulated and most controlled

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environments possible. Never before has in vivo modeling been such an integral necessity to clarifying the role of a subpopulation of cells with regard to tumor growth, progression, and resistance to therapy. The field of oncology must exhaust all capabilities in the identification of CSCs in mouse models and human patients on the chance that the now putative CSCs will soon be accepted as bona fide and responsible for a disease that has rejected most therapeutic tactics and claims a life every minute. CSCs may not ultimately be invincible.

AUTHORS' DISCLOSURES OF POTENTIAL CONFLICTS OF INTEREST

The author(s) indicated no potential conflicts of interest.

AUTHOR CONTRIBUTIONS

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